

INTERFACE AND SMALL RADIATION FIELD DOSIMETRY USING A MOSFET-BASED DETECTOR

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Abstract— Accurate dosimetry is a critical step in radiotherapy. Generally, essential dosimetric parameters are measured in a relatively flat and homogeneous water phantom, where charged-particle equilibrium (CPE) exists. However, dosimetry in certain conditions such as skin, small radiation field and interface region of two different media, CPE does not exist and therefore, poses challenges to achieve dosimetric accuracy. For accurate dose measurements in non-CPE conditions, a detector should have a small sensitive volume and water equivalent packaging to avoid dose perturbation effect. In this study, the feasibility of a MOSFET-based detector, the MOSkin detector (Fig. 1) for skin, small radiation fields and interface dose measurements were investigated. The advantages of the MOSkin detector are its water equivalent depth of 0.07 mm, small sensitive volume and water equivalent packaging.

The MOSkin detector was first characterised for *in vivo* dosimetry under megavoltage photon and electron beams. Then, the MOSkin detector was used to measure patients' skin dose in tangential breast radiotherapy and compared against dose threshold for different skin reactions. The clinical application (Fig. 2) showed that the MOSkin detector is suitable for *in vivo* dosimetry and it is necessary to accurately determine the skin dose for better clinical management of skin complications.

The suitability of the MOSkin detector in “Edge-on” orientation (Fig. 3) for small radiation field was investigated. Results showed that the MOSkin detector (Fig. 4) is suitable for dose assessment in small radiation fields as compared to other commercial detectors. The feasibility of the MOSkin detector for dosimetric verification in stereotactic radiotherapy was also tested. The result shows that it is a suitable verification tool for stereotactic radiotherapy.

Challenges in treating a lung tumour are related to respiratory-induced tumour motion and accuracy of treatment planning dose calculations in non-CPE conditions. The dosimetric characteristics near the interface of lung and Perspex media during static, respiratory-gated and non-gated (moving) radiotherapy were investigated using Gafchromic EBT2 film and the MOSkin detector in a moving phantom. In non-gated radiotherapy, dose smearing effect was observed and this effect was reduced in respiratory-gated radiotherapy (Fig. 5). However, there were still some dose discrepancies due to residual motion. The accuracy of different dose calculation algorithms near interface region was evaluated. It was found that over-estimation of the dose coverage will lead to the choice of smaller field size and thus, under-dosage to the tumour. Therefore, better dose calculation algorithms are essential.

In conclusion, the MOSkin detector has been characterised and used for dosimetric assessment in the non-CPE regions. The results suggest that the MOSkin detector possesses suitable physical characteristics for dosimetric assessment of interface and small radiation field.

Keywords— *in vivo* dosimetry, quality assurance, characterisation, stereotactic radiotherapy, skin dosimetry, electron beam dosimetry.

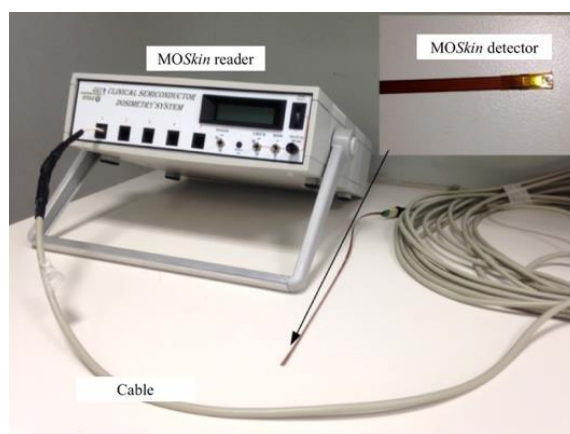


Fig. 1 The MOSkin detector system

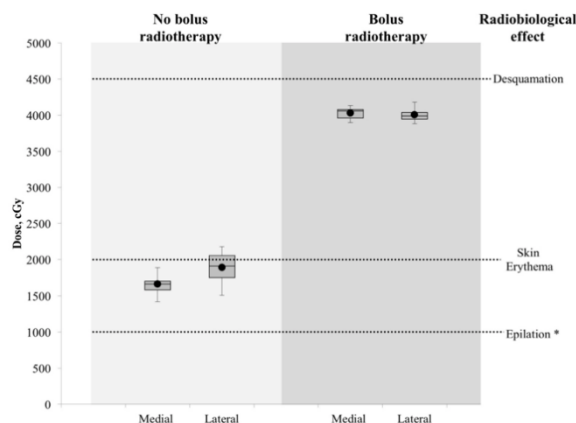


Fig. 2 Total skin dose for 13 patients who underwent “no bolus radiotherapy” and “bolus radiotherapy”. The black dots show the average total skin dose. The dotted lines show the dose threshold for different skin reactions. *This radiobiological effect does not occur on the breast but it may appear on other skin sites.

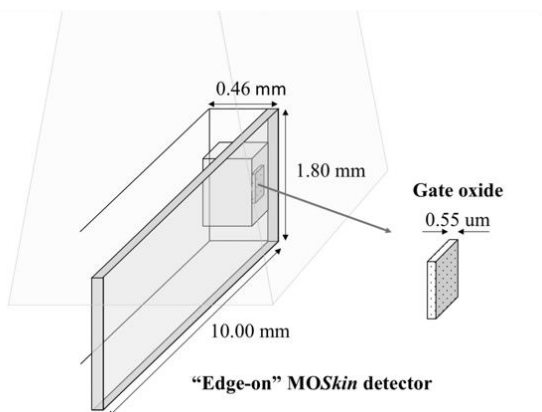


Fig. 3 The MOSkin detector in “Edge-on” orientation.

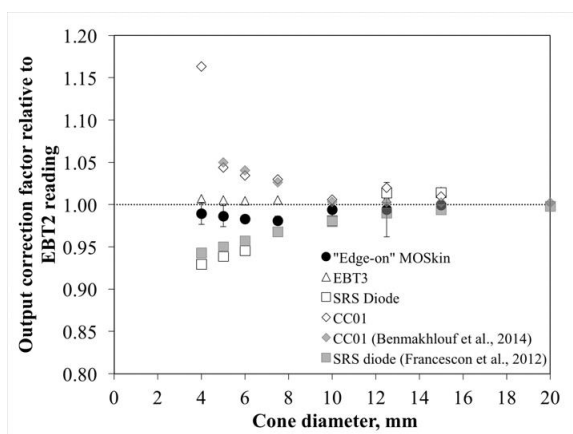


Fig. 4 Measured output correction factors for the “Edge-on” MOSkin detector and SRS diodes. All set of factors are derived from the EBT2 film measurement. The error bar shows the quadrature-combined uncertainties (1 SD) of the “Edge-on” MOSkin detector and the EBT2 film readings.

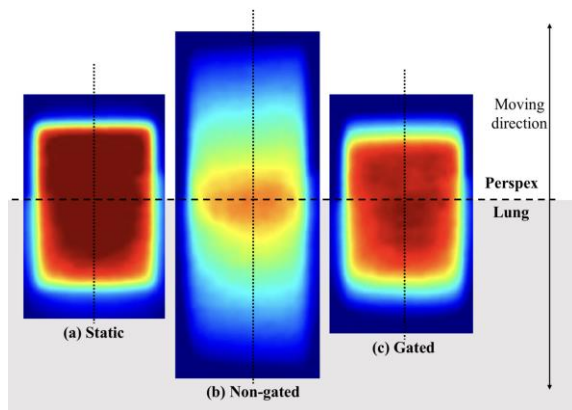


Fig. 5 Measured dose distribution using EBT2 film near the lung and Perspex interface during static radiotherapy (no motion), non-gated radiotherapy (motion amplitude of 40 mm) and gated radiotherapy with 25% gating window (motion amplitude of 40 mm).

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